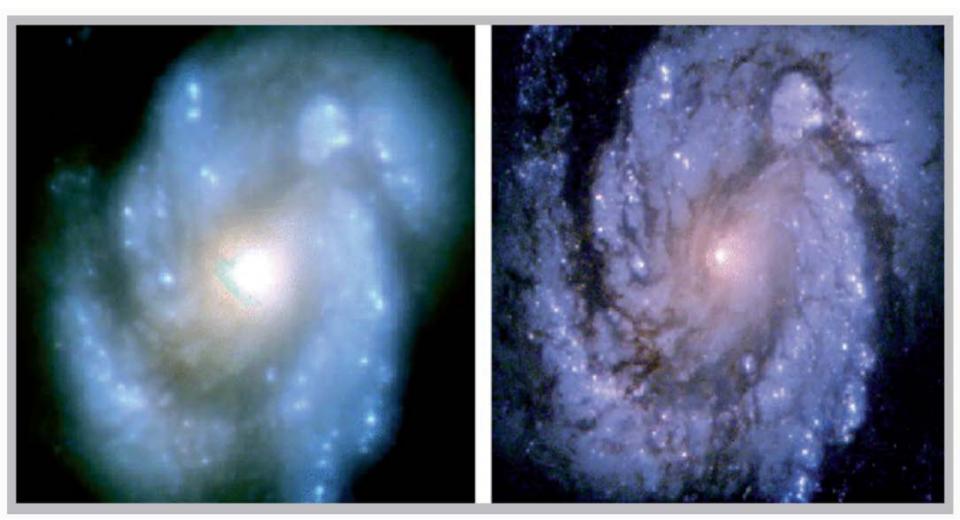
Progress Towards an International Image Quality Monitoring Framework for Quantitative Imaging

Ricardo S. Avila rick.avila@accumetra.com

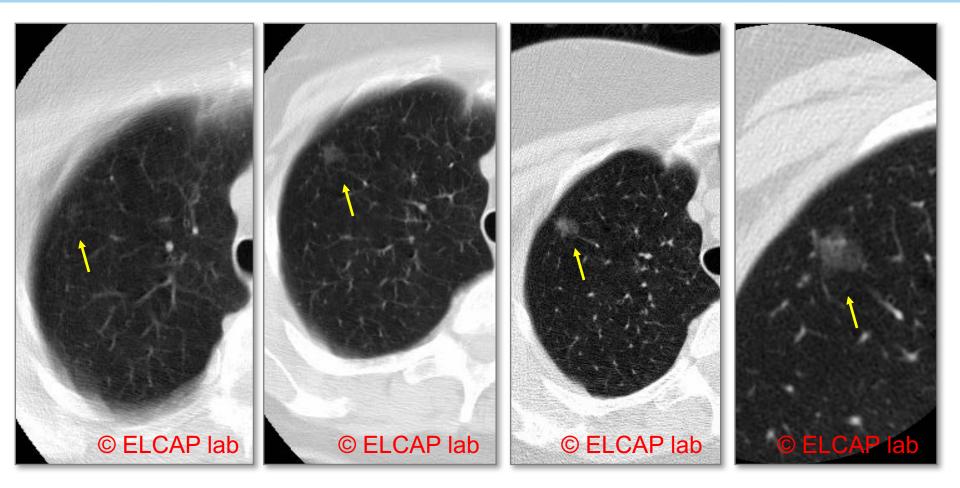
October 2, 2017

Quantitative Imaging Workshop XIV

Hubble Space Telescope



CT Image Quality



10.0 mm

5.0 mm

2.5 mm

1.25 mm

Lung Cancer Decision Support Landscape

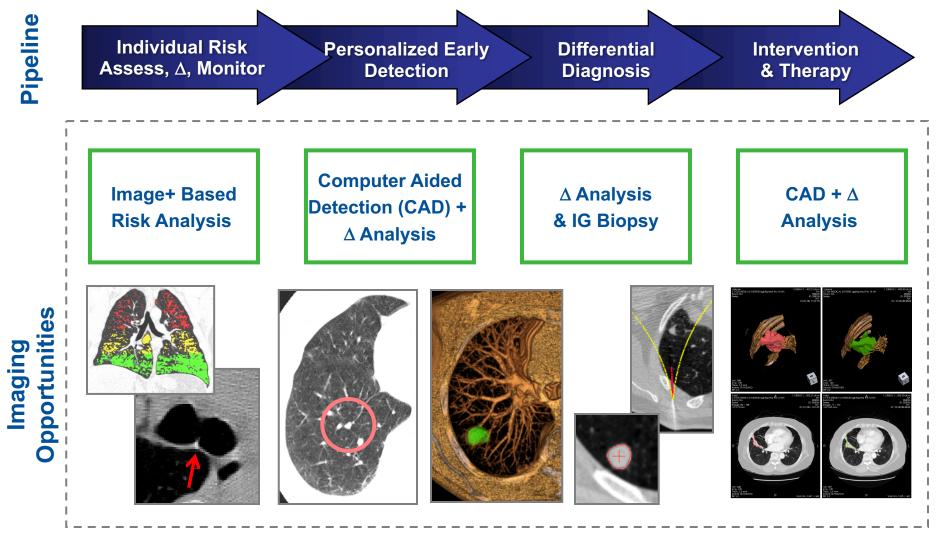
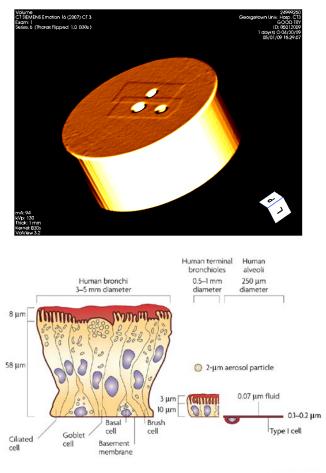
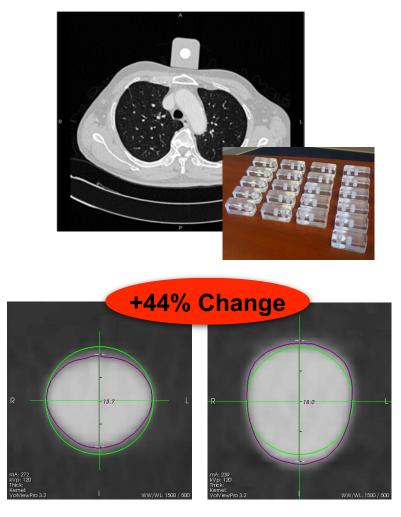


Image Quality Assessment Is Highly Task and Equipment Specific



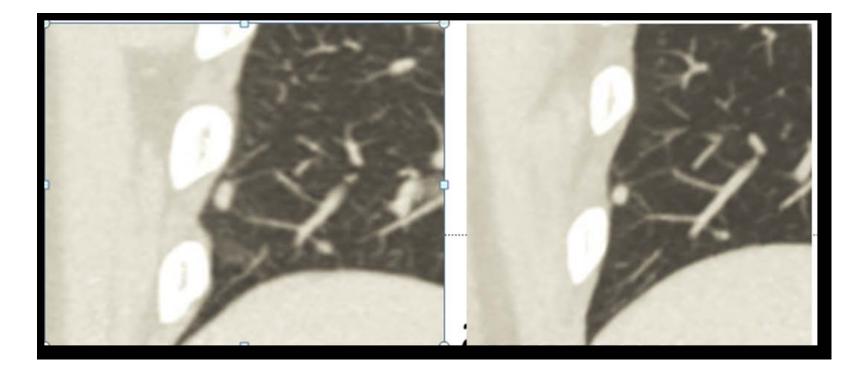
Nature Reviews | Drug Discovery

Patton and Byron Nature Reviews Drug Discovery 2007

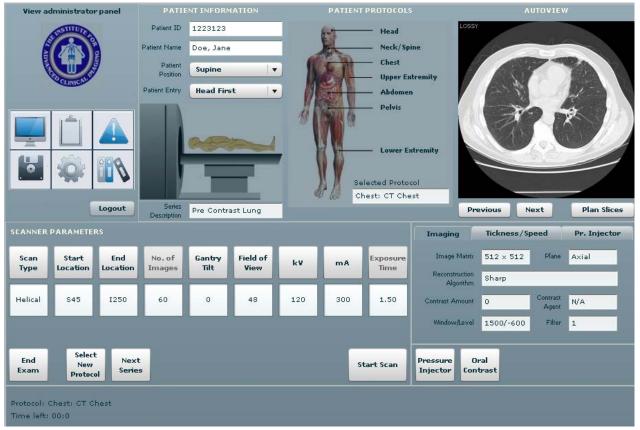


Henschke Journal of Medical Imaging 2016

Spatial Warping Example



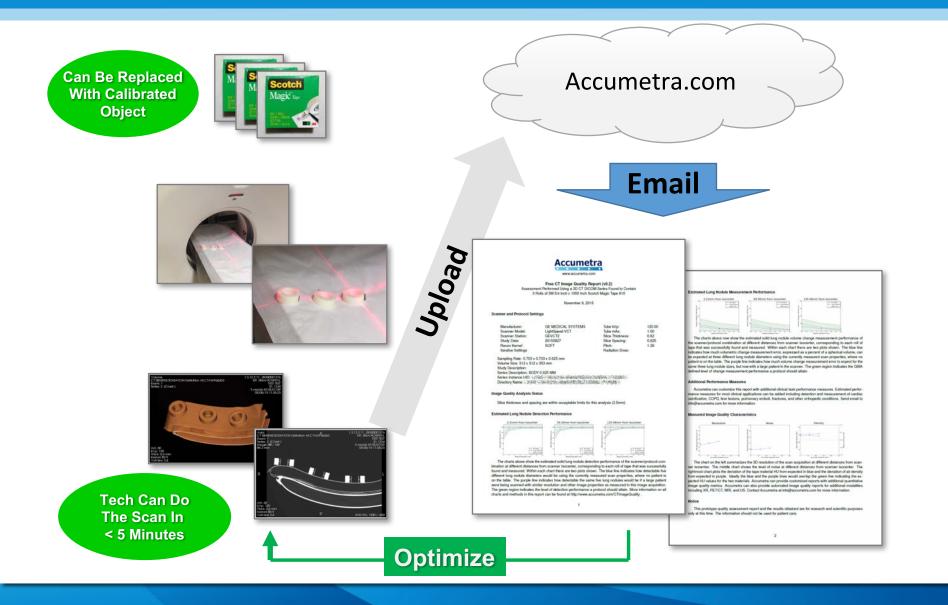
Fundamental Quantitative Imaging Problem



http://www.iacionline.com/simulators.da

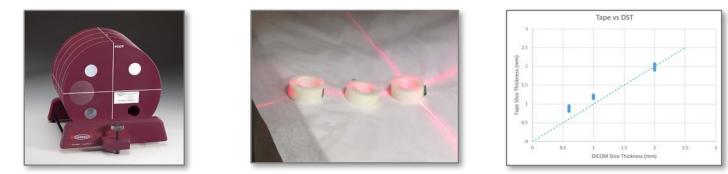
CT Scanners Have Too Many Parameter Settings And Their Tradeoffs Are Not Known

Free CT Image Quality Report

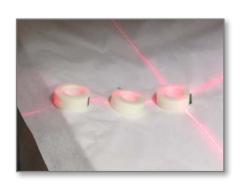


Validation Studies

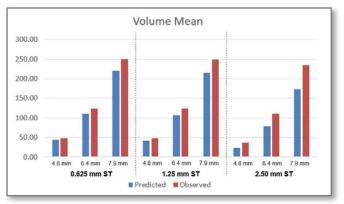
ACR Phantom and Tape Comparison



Clinical Task Prediction Performance







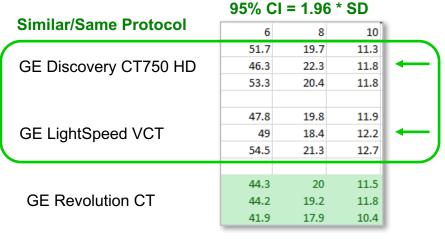
Avila SPIE Medical Imaging 2017

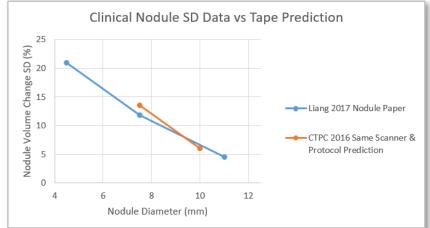
Prediction Data Point

	Cardiopulmonary Imaging • Original Research
	Variation in Screening CT– Detected Nodule Volumetry as a Function of Size
Mingzhu Liang ^{1,2} Rowana Yip ¹ Wei Tang ^{1,3} Dengming Xu ¹ Anthony Reves ⁴ Chudia I. Henschke ¹ David F. Yankelevitz ¹	OBJECTIVE. The objective of this muly is to evaluate measurement variability in volu- metic assessment of palmonary nodules on low door CT manyes with a view toward doer imming bow this variability in influence by nodule area. MATERIALS AND METHODS. A large CT accreming database was reviewed to iden thy vold palmonary nodules that had warmade stables in the on the basis of buildings from a least three scans obtained over a 3-year period. Two software packages dang VCAR and nys pavod were usualized in a scene the toolky obsame on the post of scenes and the scenes obsamed over a 3-year period. Two software packages dang VCAR and nys pavod were usualized as a scene the toolky obsame on the post of scenes and the scenes of the software obsame of the scenes of the software obsamed of the scenes of the scenes of the software obsamed of the scenes of the software obsamed of the scenes of the scenes of the scenes of the software obsamed of the scenes of the scen
Reywords: measurement error, nodule volumetry, someoning, variability	creating nodule diameter, with the use of both software packages. CONCLUSION. Measurement variability decreased with increasing nodule diamete for both software packages and was different between the two software packages.

TABLE 2: Percentage of Volume Variation Between Software Packages, by Nodule Size

Software Package and Percentage of Volume Variation	< 4 mm (<i>n</i> = 83)	4–5 mm (<i>n</i> = 62)	6–9 mm (<i>n</i> = 20)	≥ 10 mm (<i>n</i> = 6)		
Lung VCAR ^a						
Mean ± SD	-2.3 ± 20.4	4.7 ± 17.7	1.5 ± 14.6	0.3 ± 3.7		
Median (IQR)	-4.8 (-18.4 to 11.1)	6.1 (-7.3 to 16.7)	1.4 (-4.5 to 9.0)	-0.2 (-0.5 to 3.7)		
syngo.via ^b						
Mean ± SD	9.7 ± 59.5	-1.7 ± 24.3	-1.0 ± 9.1	4.9 ± 6.2		
Median (IQR)	0.0 (-20.7 to 25.0)	-0.5 (-15.0 to 13.8)	1.0 (-5.2 to 4.2)	5.7 (0.7-8.7)		
Note—IQR = interquartile range. ªVersion 11.3–10.11, GE Healthcare. bVersion VA20, Siemens Healthcare.						

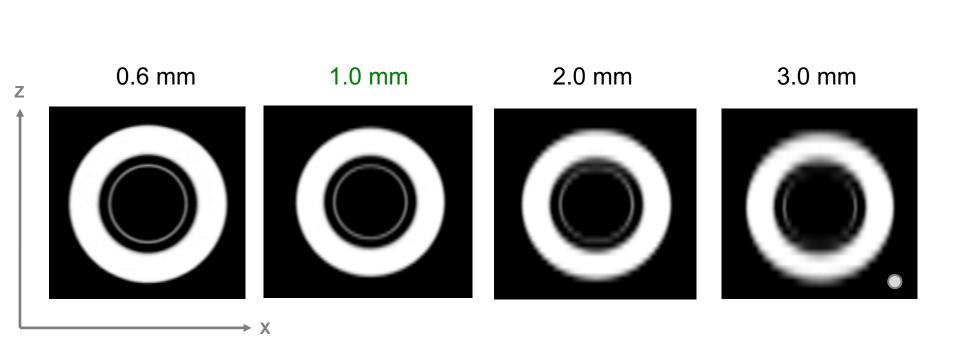




Detection Slice Thickness & Recon Kernel

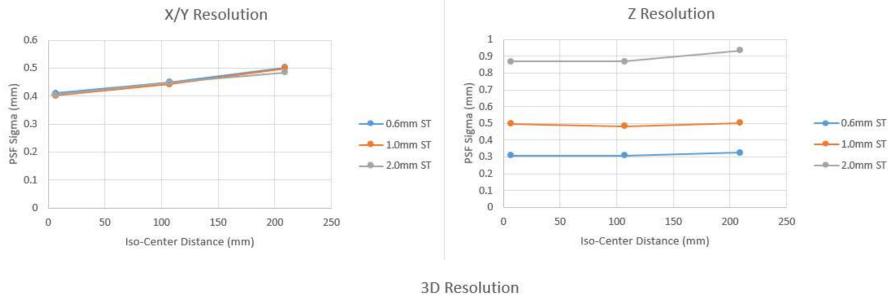
Slice Thickness			Medium Recon	Edge En. Recon
<= 0.625	4 (15%)	0	3	1
0.8, 1.0, 1.25	12 (46%)	6	2	4
>= 1.5 3 used 2mm ST & 1mm spacing	10 (38%)	6	3	1

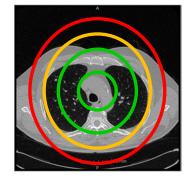
Need To Control CT Slice Thickness (Resolution)

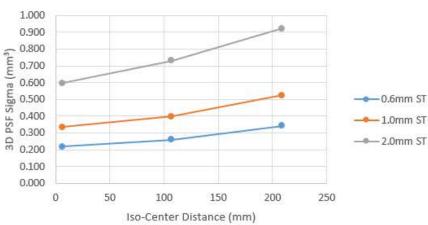


WW = 1000 WL = - 400

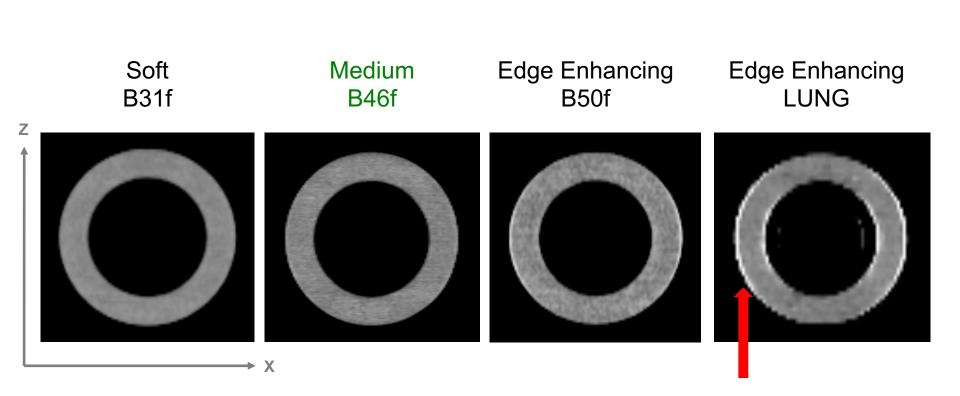
3D Resolution





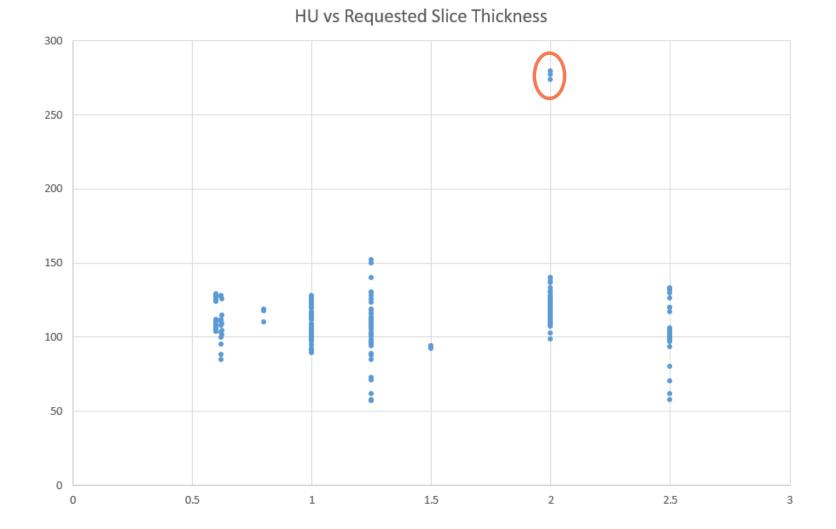


Need To Control For Edge Enhancement (and Resolution)

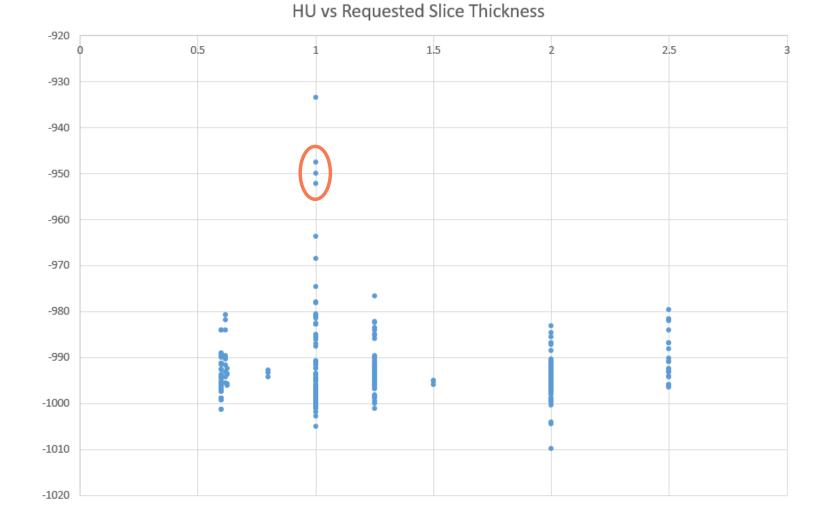


WW = 400 WL = 100

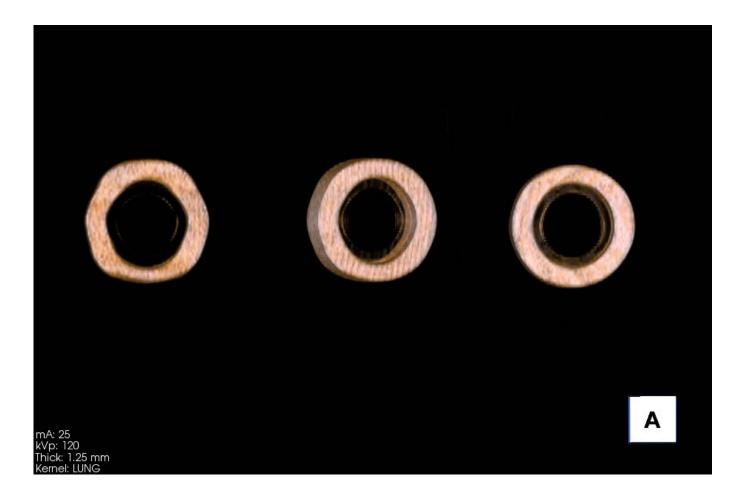
Need To Control For HU Bias - Tape



Need To Control For HU Bias - Air

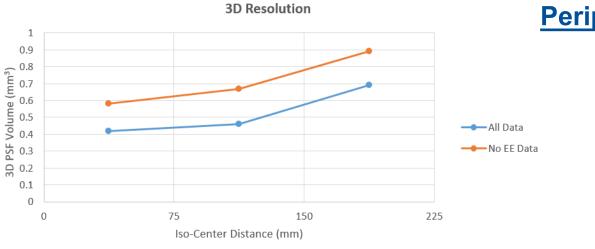


Need To Control Z Spatial Warping



Results For <= 1.25mm Slice Thickness

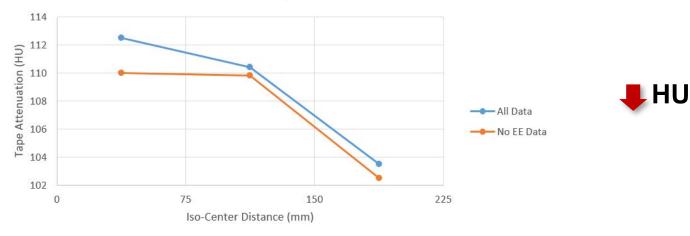
2017 WCTI Hot Topic Abstract



Periphery Implications



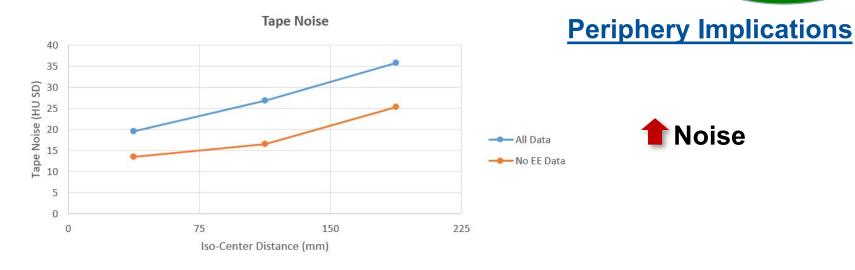
Mean Tape HU



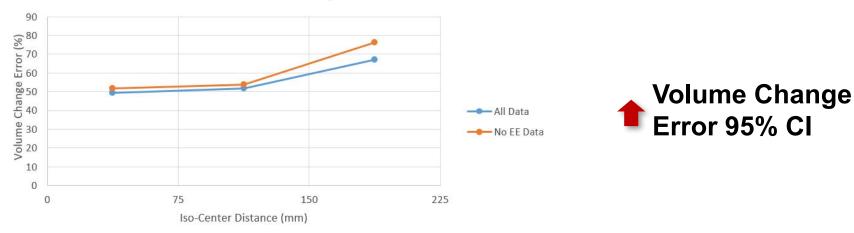
Results For <= 1.25mm Slice Thickness

2017 WCTI **Hot Topic** Abstract

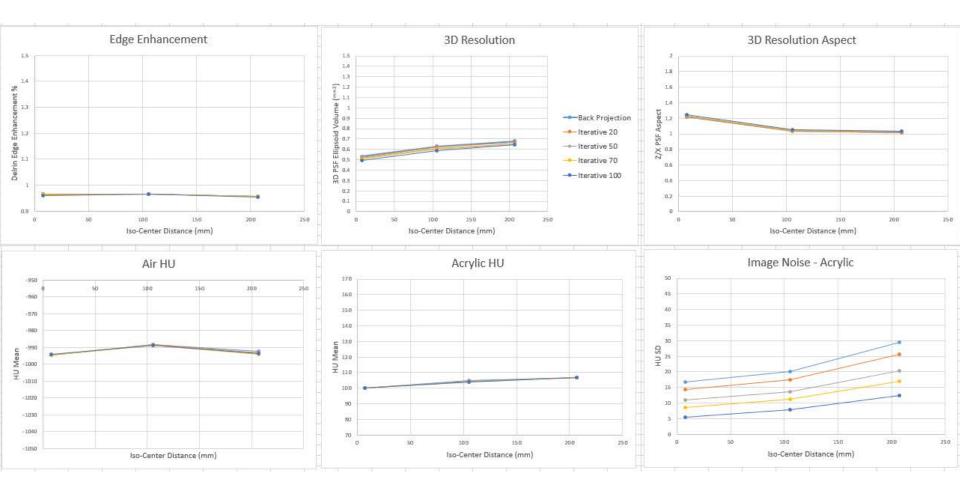
Noise



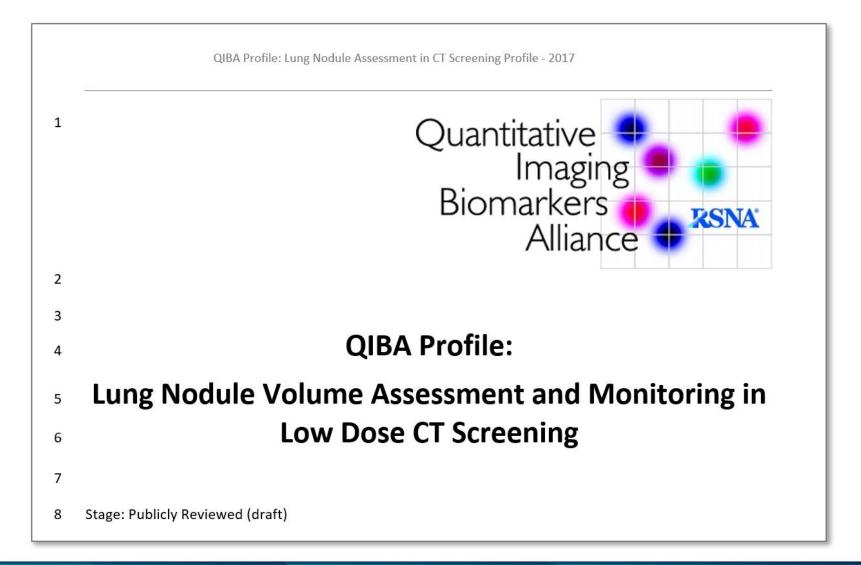
6mm Solid Nodule Volume Change Error 95% CI



Impact of Iterative Reconstruction



QIBA CT Lung Nodule Profile



Our Smallest Target



Profile Requirements & Steps

CT Scanner

- >= 16 Slice
- Model has been verified to be QIBA Compliant
- ACR CT accreditation

CT Protocol

- <= 1.25mm slice thickness</p>
- Slice spacing <= slice thickness
- Medium reconstruction kernel
- Pitch < 2.0

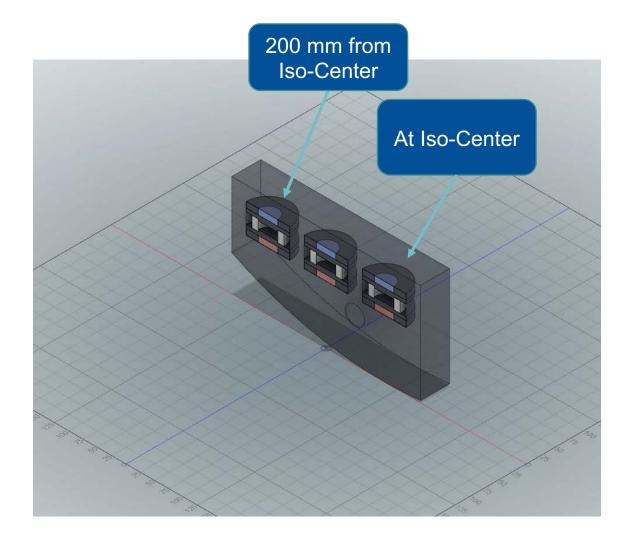
. . .

Verification is Challenging For Many Clinical Sites

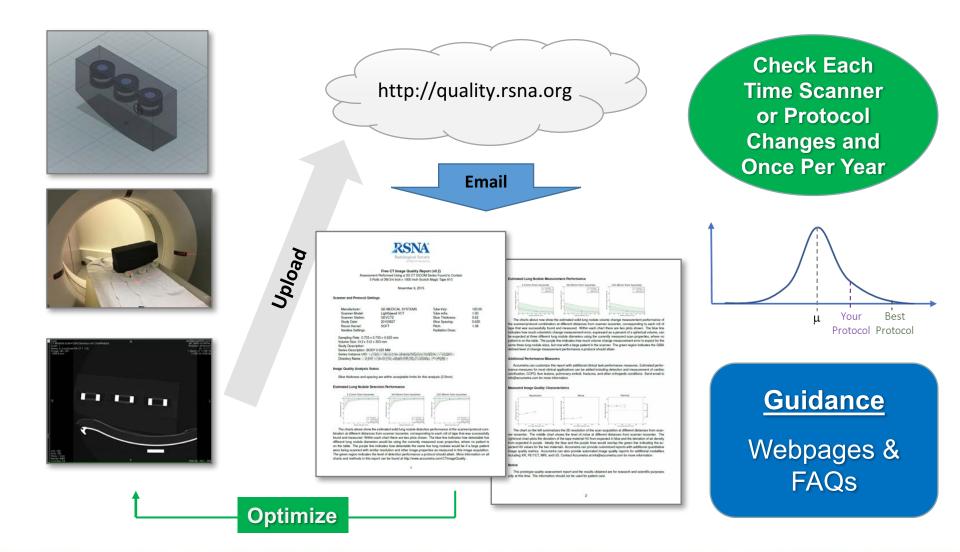
- Fundamental Image Properties
 - Edge Enhancement <= 5%</p>
 - 3D PSF Ellipsoid Volume
 <= 1.5mm³
 - 3D PSF Aspect <= 2.0</p>
 - HU Bias < 35 HU</p>
 - Spatial Warping RMSE <= 0.1 mm
 - Image Noise <= 50 HU SD</p>
- Nodule Analysis
 Software

ftware has been verified be QIBA Compliant

CTLX1 Phantom



QIBA Pilot: Conformance Testing



Anthropomorphic Phantom Testing of the CTLX1 Phantom

Preliminary Results



CT Scanning Study - Siemens

CT Scanner:

Siemens Somatom Definition AS

Main Protocol:

Low Dose Lung Cancer Screen QIBA SN Profile Conformant

Protocol Variants:

0.6 mm B40f (blue lines) 1.0 mm B40f (orange lines)

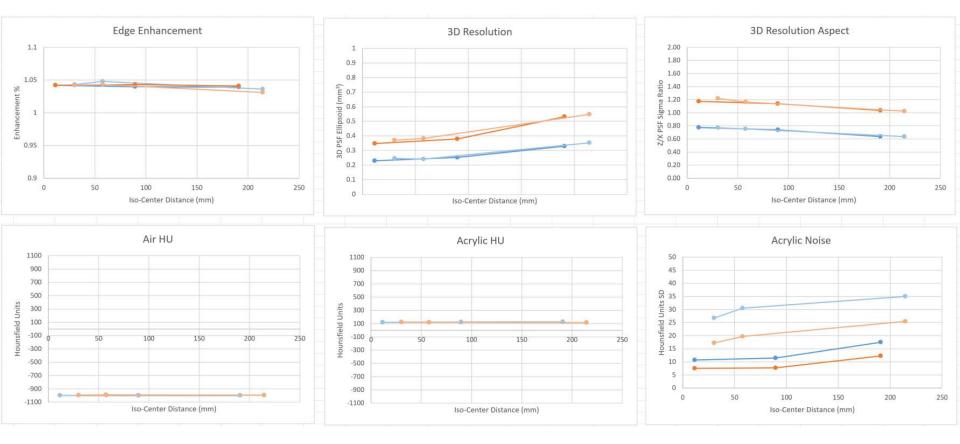
Phantoms:

- 1) CTLX1 Phantom (darker color)
- 2) Anthro Chest Phantom w/ CTLX1 Phantom modules (lighter color)

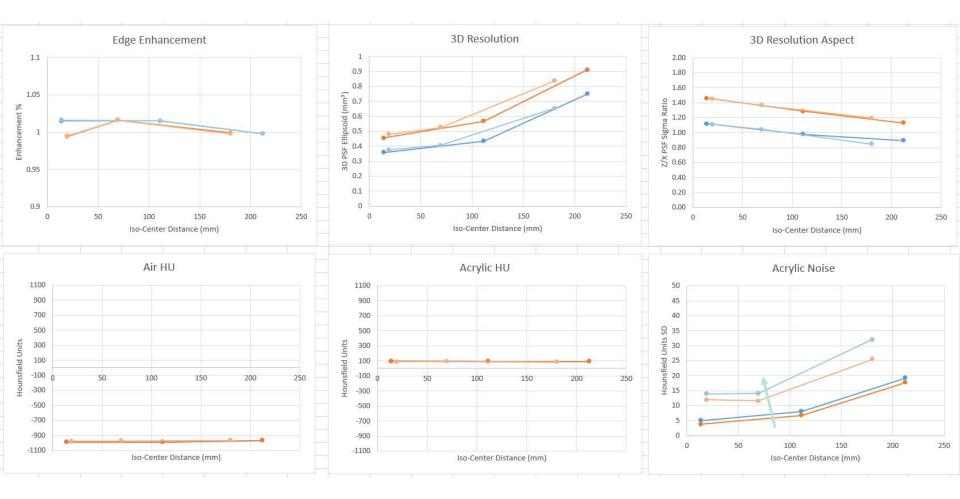
Measurement:

Fully Automated Accumetra SW

Preliminary Results - Siemens



Preliminary Results - GE



CT Scanner and Software Vendors

CT Scanner DOE

Provide Recommended CT Scanning Protocol

Test the Protocol Over an Operating Envelope

[Insert The Following As A Table	
mAs	40
<u>kVp</u>	100
Rotation Time (s)	0.50
Filed of View (cm)	35.0
Pitch	1.50
Slice Thickness (mm)	1.00
Slice Spacing (mm)	0.75
Reconstruction Kernel	140-4
Table Height	Centered

Will have a DOE with the following 19 experiments consisting of 3 repeat CT scans of the recommended CT acquisition protocol (A,B,C) and 16 CT scans that systematically vary <u>mAs</u>, FOV, Pitch, and an iterative reconstruction setting:

[Insert The Following As A Table

1

Experiment #	mAs	FOV	Pitch	Iterative Recon Setting	Notes
Α	40	30.0	1.50	140-4	Repetition 1
01	30	30.0	1.25	140-3	[-, -, -, -]
02	30	30.0	1.25	140-5	[, -, +]
03	30	30.0	1.75	140-3	[, +, -]
04	30	30.0	1.75	140-5	[-, -, +, +]
05	30	40.0	1.25	140-3	[-, +, -, -]
06	30	40.0	1.25	140-5	[-, +, -, +]
07	30	40.0	1.75	140-3	[-, +, +, -]
08	30	40.0	1.75	140-5	[-,+,+,+]
В	40	35.0	1.50	140-4	Repetition 2
09	50	30.0	1.25	140-3	[+,, -]
10	50	30.0	1.25	140-5	[+, -, +]
11	50	30.0	1.75	140-3	[+, +, -]
12	50	30.0	1.75	140-5	[+, -, +, +]
13	50	40.0	1.25	140-3	[+, +, -, -]
14	50	40.0	1.25	140-5	[+, +, -, +]
15	50	40.0	1.75	140-3	[+, +, +, -]
16	50	40.0	1.75	140-5	[+, +, +, +]
С	40	35.0	1.50	140-4	Repetition 3

CT Scanner and Software Vendors

- Analysis Software Vendors
 - Scans of well characterized synthetic and clinical zero change datasets will be provided
 - We will check for near zero bias from 6mm to 12mm diameter solid lesions
 - We will check that the analysis software does not exceed the CV table provided in the profile

We Are Now Distributing 80 CTLX1 Phantoms & Launching New Quality Monitoring Services

- 40 CTLX1 Phantoms Will Be Distributed To Lung Cancer Screening Sites Outside of the United States
- Another 40 CTLX1 Phantoms Will Be Distributed To Lung Cancer Screening Sites In the United States
- Working With RSNA/QIBA We Are Piloting The 1st Small Nodule Change Measurement Conformance Service
- Launching The New 2017 CT Lung Imaging Protocol Challenge Here
- Funding Thanks To The Prevent Cancer Foundation

International CT Image Quality Monitoring

- Monitoring Infrastructure
 - Ultra-low cost CT phantoms requiring <= 5 min to scan
 - Web-based Analysis Tools and Calculator(s)
 - All Running on the Amazon Web Services (AWS) cloud



Challenges

- Getting the Word Out To Sites
 - We need champions (RSNA/QIBA, Advocacy, etc)
- International Regulations
 - Who can help navigate?
- Support For More Application Areas Increases Cost
 - More materials, higher overall mass, and added algorithms
 - Some solutions increase complexity and scanning time
- Thinner Slices = More Review Time
 - We must get Radiology to accept the routine acquisition of multiple scans with at least one high res scan for algorithms
- Continuously Changing CT Technology
 - Iterative Reconstruction Algorithms

Potential Benefits of Improving Global CT Image Quality Through Site Optimization & Correction

- Improved Earlier Lung Cancer Detection : 4mm
- Improved Differential Diagnosis: Improved Sens/Spec
- Shorter Follow-Up Times: 1 to 2 Month Follow-up
- Improvements to Existing Biomarkers: New Sub-Types
- New Biomarker Discoveries: ?

QIW Recommendations

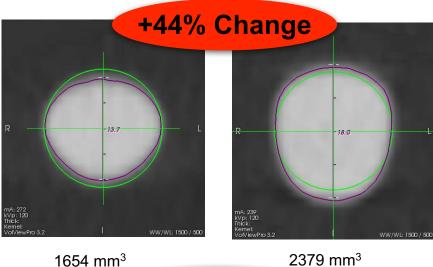
- Allow Clinical Sites to Acquire At Least One High Resolution CT Lung Screening Scan That Is Intended Only For Computational Analysis
- Encourage CT Scanner Manufacturers To Support 1024x1024 Matrix Size and Clinical Sites To Use It For Computational Analysis
- Enable Reimbursement For Quality Verification of Scans

Thank You

2010: Roche ABIGAIL Study

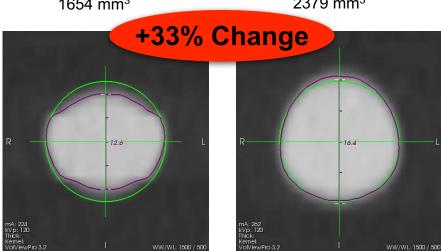


Model A Site 1





Model A Site 2



1601 mm³

2127 mm³

Understanding Lung Nodule Volumetric Error

